# Automatic Screening of Retinal Lesions for Grading Diabetic Retinopathy

Muhammad Sharif<sup>1</sup> and Jamal Hussain Shah<sup>1,2</sup> <sup>1</sup>Department of Computer Science, COMSATS University Islamabad, Pakistan <sup>2</sup>University of Science and Technology of China, China

Abstract: Diabetic Retinopathy (DR) is a diabetical retinal syndrom. Large number of patients have been suffered from blindness due to DR as compared to other diseases. Priliminary detection of DR is a critical quest of medical image processing. Retinal Biomarkers are termed as Microaneurysms (MAs), Haemorrhages (HMAs) and Exudates (EXs) that are helpful to grade Non-Proliferative DR (NPDR) at different stages. This research work contributes an automatic design for the retinal lesions screening to grade DR system. The system is comprised of unique preprocessing determination of biomarkers and formulation of profile set for classification. During preprocessing, Contrast Limited Adaptive Histogram Equalization (CLAHE) is utilized and Independent Component Analysis (ICA) is extended with Curve Fitting Technique (CFT) to eliminate blood vessels and optic disc as well as to detect biomarkers from the digital retinal image. Subsequent, NPDR lesions based distinct eleven features are deduced for the purpose of classification. Experiments are performed using a fundus image database. The proposed method is appropriate for initial grading of DR.

Keywords: DR, CLAHE, ICA, CFT, biomarkers.

Received December 10, 2015; accepted March 24, 2016

# **1. Introduction**

Diabetes is a quickly expanding disease on the planet [49]. In Pakistan alone; over 6.2 million people having Diabetic Retinopathy (DR) type disease are already at the risk of becoming blind [16]. Diabetes is not diagnosed in large number of people, which may leads to blindness. Diabetes damages sensitive tissues retinal blood vessels causing blindness [51]. Many problems can follow diabetes, one of which is DR, resulting complete blindness. A diabetic Mellitus triggers DR, which is an eye vulnerable sickness. It affects the retina of the eye. It is categorized into four phases with respect to severity level; mild non-proliferative DR, moderate Non-Proliferative DR (NPDR), severe NPDR and proliferative DR. Long-term diabetes is said to be a primary cause of DR which causes permanent vision loss. This disease occurs in steps. Patient does not feel any sign of visual weakening at the early phase. The wounds existing on the retina determines the concentration of DR.

A human retina is comprised of several parts for example blood vessels, macula, fovea and the optic disc. There are two phases of classification for the DR; NPDR and Proliferative DR (PDR). On the injury of the blood vessels in retina, a fluid starts to be discharged. Consequently, retina turns into wet and swollen. At this phase, several identifications of retinopathy persist. For illustration, Hemorrhages (HMAs), Microaneury'Sms (MAs), Exudates hard as well as soft (EXs) and Inter-Retinal Microvascular Abnormalities (IRMA). The growth of new erratic blood vessels in retina produces PDR. PDR may cause complete blindness [31] as it is the last phase of DR. The problem in DR yields Diabetic Macular Edema (DME) which is the basis for the blindness [48]. A diabetic is a communal sickness. Here, pancreas fails to produce adequate insulin. As an outcome of which unmanagable glucose level arises in the body. This constant glucose level results problem in the eye termed as diabetic retinopathy [12]. This illness happens because of microangiopathy which disturbs different regions of the eye:

- 1. Capillaries.
- 2. Venues.
- 3. Arterioles. There are two primary reasons for this retinal injury:
  - 1. Microvascular blockage.
  - 2. Microvascular leakage.

With the increase of blood glucose level, changes in the retinal blood vessels are sparked, resulting retinopathy [29, 44]. Accompanied by microvascular blockage and leakage, occassionally development of anomalous fresh blood vessels on the retinal surface is a reason for the retinopathy. The existence of MAs in the eye is initial indication of retinopathy. Previously, victim does not sense any DR. This may advanced to permanent damage of sightedness. Atypically, both eyes are influenced by DR [28]. Also, alteration hapens in the mass of blood vessels (swelling) Microaneurysm, Exudates, Hemorrhage along with new blood vessels develop. Earlier detection of such changes helps in the selection of further treatement steps [43]. Exudates are the primary signs of DR and the primary cause of blindness. Early screening process can help restrain its development. In this paper, the symptoms mentioned above of DR will be considered, and an automated system for screening of DR at early stages will be presented.

Mostly, the principal reason of DR is visual disability. Fundus images DR images helps to diagnose the disease. DR can be significantly be identified by the use of digital images. Different color spaces can be determined is the segmented region. An economical Computer Aided Diagnosis System (CAD) is used in this research work. Blood vessels, optic discs and Exudates in the digital fundus images are extracted. Exudates are identified as the combination of protein and lipid in the retina. They color is white or cream. Bright lesions and reflection is observed on Exudates. They signify associated hazards of retinal edema or swelling. Elimination of retinal constituents identified as vessel tree and optic disc is primary important step. Exudates residents are emphasized after detachment of other structures.

With the growth in the sum of DR patients', CAD obtained significant recognition because of slow work of traditional analysis of fundus images. Literature regarding CAD system for DR grading pertains differences, we will consider DR grading methods based on biomarker as discussed earlier. By using the CAD system, noteworthy analysis has been performed to identify the DR from fundus images. Researchers selected various biomarkers to determine vascular diseases. These vascular based identification systems are discussed in [4]. A biomarker related to vascular is employed. A grading system is thrived out of it.. Likewise, other biomarkers comprise retinal MAs [10, 37], EXs [11, 25], HMAs [18, 37], distances between the EXs and fovea to plan a ranking system for the disease. Using the stated image based biomarkers, numerous ranking or grading systems incorporates mutual assessment of versatile features. After feature extraction, researches determine the level of DR with the help of a classifier such as Raia and Vasuki [34] analyzed the EXs at fovea region to classify the normal and abnormal DR images while classification is achieved by Support Vector Machine (SVM). in the same way, classifier based DR grading system is presented by Tariq et al. [45] in which authors extract fifteen different features based on Exs, MAs, and HMAs. Microaneurysm based automatic DR screening system is introduced in [5]. Murray et al. [27] introduce Real-time screening system build on Amplitude Modulation Frequency Modulation (AM-FM) automated grading system. In this system, authors extract the retinal features and classify fundus images into two classes' namely normal or abnormal grade using supervised learning. Klein et al. [21] also introduced a system in to monitor DR progression by analyzing changes in the diameter of retinal vessels. Similar, retinal vessel segmentation discussed in [6].

Contextual information is vital in medical images. Contextual data is employed for the discovery and distinguishability of bright lesion in the retinal image. Contextual data is also used to identify coronary classification and hard exudates in the CT scan images [9, 38]. Hashim and Hashim [13] performed on contextual information at image level for automatic screening on DR. Although the advantages of the CAD mentioned above system are used systematic analyzes with the same purpose, still need more improvement to diagnose DR at an early stage.

This paper investigates automatic grading system for the recogonition and classification of DR at different levels. In the proposed system, Curve Fitting Technique (CFT) based on thresholding is introduced for lesion extraction. Moreover, eleven potential features based on NPDR lesions are extracted and ensemble for classification purpose. More detail of proposed system is discussed in the upcoming sections.

# 2. System Overview

There are two phases of DR; detection and classification. Fundus digital images are used by the DR to identify all disease signs. Biomarkers are then extracted. This research emphasized on the stage wise detection of EXs and Mas for grading of DR. The new system has the stages named candidate region preprocessing with feature extraction and DR grading. Figure 1 identifies the flow of our proposed work.



Figure 1. Flow diagram of our system.

### 2.1. Candidate Region Preprocessing

Biomarkers above are dependent on the quality of images taken from different modalities. A lot of work has been done by researchers since the last two decades to enhance the images quality so that the ophthalmologists can quickly determine abnormalities from them. The performance of DR detection techniques depends on image processing algorithms like enhancement and segmentation of images [24] to extract useful information. These techniques are also utilized to enhance the visuals of images. Also, it is essential to improve low contrast data of retina blood vessels with respect to the background. Otherwise, it 's hard to extract the abnormalities. Some enhancement methods were used such as histogram equalization and other enhancement techniques to improve the contrast of images [17, 36]. Contrast stretching is one of the essential image enhancement techniques. Most common contrast stretching techniques are based on local and global contrast [46], partial contrast [23], bright and dark contrast [14]. Nowadays DR detection at the premature stage is a challenging area of medical image processing.

In the proposed system, two techniques namely CLAHE [50] and ICA [1] are utilized for local and global enhancement. CLAHE is a small window built method which is utilized to improve the distinction of retinal blood vessels with reference to its background keeping the bright and dark areas in perspective. It further improves the vessels in changing environment uniformly, and it is an extended technique of histogram equalization and contrast stretching [33]. The main reason of utilizing CLAHE is to apply it on small tiles obtained by dividing the image into small window's image. Grey level values are uniformly dispersed earlier inside the window to confirm an observable concealed structure. Mean filter using CLAHE is used to improve the fundus image. This identifies the vessel. Later, bottom-hat morphological transformation is applied to eliminate the retinal vasculature. Background noise elimination is done through contrast stretching to decrease surplus line structures.

Let  $\phi_{d\min}$  and  $\phi_{d\max}$  be termed as least and maximum intensity values that can be described mathematically as:

$$h = 255 * \frac{\left[\Theta_s(\phi_d) - \Theta_s(\phi_{d\min})\right]}{\left[\Theta_s(\phi_d\max) - \Theta_s(\phi_{d\min})\right]}$$
(1)

Where,  $\Theta_s$  is known as sigmoid function and  $\phi_d$  represents the dark or bright regions respectively. Sigmoid function  $\Theta_s$  can be defined as:

$$\Theta_s(\phi_d) = \left[1 + \exp(\frac{\varpi_s - f}{\sigma_s})\right]^{-1}$$
(2)

Where,  $\sigma_s$  and  $\sigma_s$  represents the mean and variance of intensity values respectively.

ICA is a method to examine innovative signals from the combinations of numerous self-determining sources [11, 18]. Here low contrast enhancement in fundus image is done by ICA for retinal pigment structure, i.e., hemoglobin, muscular pigment, and melanin. Figure 2 shows the result of preprocessing fundus image.



Figure 2. Candidate region preprocessing.

### 2.1.1. Vessel Extraction

After enhancement, next phase is to determine the blood vessels and eliminate it from the candidate region. It is a very sensitive process because it can eliminate or introduce clinical information that can be helpful or dangerous in clinical patient screening for DR grading. For this purpose, matched filter is applied that uses Gaussian curve [41]. Blood vessels contain low contrast intensity values which require extra enhancement. Consequently, a matching of 2-dimensional filer with the kernel is needed. This convolves the original image. It can be defined as:

$$I(u, v) = -\exp(-\frac{u^2}{2\sigma^2}), \text{ for } |v| <= L/2$$
 (3)

Here, L is the length of the segment along y-axis where vessels are considered to have constant orientation. Then the thresholding technique is employed to extract the blood vessels. Figure 3 depicts the outcomes of blood vessels recogonition.



Figure 3. Preprocessed image and respective blood vascular pattern.

#### 2.1.2. Optic Nerve and Macula Detection

The localization of retinal landmarks in particular Optic Nerve Disk (OND) plays an important role to correct pathological conditions of DR in the CAD system. The brightest region in the retinal fundus image is OND. OND contains three unique properties for its localization:

1. It appears as the highest intensity value having approximately 1600m in diameter.

- 2. Arteries and veins enter and leave from it.
- 3. Blood vessels also depart from here.

The following Equation calculates the central mass of OND:

$$x_i = \frac{\sum_{i=1}^{m} x_m}{m} \quad y_i = \frac{\sum_{i=1}^{m} y_n}{n} \tag{4}$$

On the other hand, the macula is the darkest region located near to OND and approximately in the center of the retina. It is a sensitive retinal area and liable for thorough pivot vision. Classification related to retinal abnormalities is essential to identify the pivot region of macula which is known as the fovea. Much work has been carried out to identify the area of macula [26, 33]. In the proposed system, simple thresholding technique is extended to eliminate macula subtraction. Figure 4-a and Figure 4-b show the marked selection of OND and macula and segmentation of OND respectively.





Figure 4. Optic nerve disk preprocessing, segmentation and lesion selection.

## 2.1.3. Lesion Segmentation

The key marks of NPDR are called Exudates. It is the ruling starting point of blindness. Early screening process helps to prevent this problem. The growth of protein and lipid in the retina create EXs which are white or cream color bright lesions [42]. Additional MAs is also the significant biomarkers of NPDR and is started by the principle dilatations of thin vessels of the blood. MAs are of minor dimensions, nearly red in color and round. The difference of MAs and HMAs is minor bright red dots and larger bright red dots respectively. In this paper, the first average threshold for N DR affected images is selected manually, and the

algorithm successfully detected the biomarkers mentioned above. Then, the statistical CFT is utilized to compute the minimum intensity value for the detection of biomarkers. The CFT is defined as follows:

$$f(x) = p1^* x + p2$$
(5)

Where x is the highest intensity in the processed image and-and p2 are the constant coefficients having 95% confidence boundary. The binary lesion segmentation for MAs, HMs, and EXs extracted from processed image is defined as:

$$I(x, y) = \begin{cases} 1, & I(x, y) > f(x) \\ 0, & I(x, y) < f(x) \end{cases}$$
(6)

Where, I(x, y) is known as intensity value of fundus image. Figure 4-c shows the segmentation of lesion.

## 3. Feature Extraction and DR Grading

Normal, mild, moderate and severe DR is used by different works for automated classifications of fundus images [8]. Commonly, fundus images are further categorized by different authors into two, three, four and five classes. In a two class, the images are normal and NPDR whereas Normal, PDR, and NPDR are for three class classification. On the other hand, for four classes, the categories are normal, moderate NPDR, severe NPDR and PDR whereas normal, mild DR, moderate DR, severe DR and PDR are for five class classifications.

In this paper, four class classifications of fundus image are used which are normal, mild, moderate and severe DR. For the classes above; it is essential to extract significant features for accurate screening. In this regard, the candidate region is divided into three rectangular shape areas in the center of the macula. To form a feature set, the following feature set is ensemble for accurate classification.

• f1-f3: Calculations of mean, standard deviation and sum of each pixels values of every part.

$$f_{1} = \sum_{i=1}^{N} I(x, y)$$
(7)

$$f_2 = \frac{J_1}{N} \tag{8}$$

$$f_3 = \frac{1}{N} \sqrt{\sum_{i=1}^{N} (I_i(x, y) - f_2)^2}$$
(9)

- f4-f6: Count number of EXs, H and MAs in each part.
- f7: Convert original fundus image into HSV color space and calculate the mean value from inside of candidate region.
- f8-f10: Sum of the difference of EXs, H, and MAs with a manually selected trained value of EXs, HMAs, and MAs from inside of candidate region.

• f11: Calculate the cross-bin distance from the average trained value of macula region. It can be defined as follows:

$$f_{11} = (h_{macula} - h_{avgTrained})^T W (h_{macula} - h_{avgTrained}$$
(10)

Where  $W=[x_{ij}]$  is the weight matrix and  $[x_{ij}]$  represents the similarities between bins.

Let F be the features set to represent the candidate region. It can be defined as:

$$F = \{f_1, f_2, f_3, \dots f_n\}, \text{ where } n = 11$$
 (11)

Consider, *C* illustrates the class representation and  $\{C_i | i = 1, 2...n_C\} \in \mathbb{R}^D$  is the *i*<sup>th</sup> class where  $n_C$  shows the total number of classes.

Therefore in the first step, the data is classified into two stages which are normal and severe. Severe stage arises by the accumulation of exudates around macula region which is classified by using Gaussian Bayes classifier [39]. This classifier optimality detects the severe stage DR based on MAs and EXs. It can be written as:

$$p(c \mid y, X) = \frac{p(y \mid X, c) * p(c)}{p(y \mid X)}$$
(12)

Where, *X* represents the combination of f1-f6 input feature vector to classify the severe stage DR or non-severe stage DR, y represents the observed target value and p(c) is known as prior class p(y | X, c) which can be expressed as:

$$p(\mathbf{y} | \mathbf{X}, c) = \int p(\mathbf{y} | \mathbf{X}, c) p(c) d_c$$
(13)

Also, to observe severe stage of DR, the central part of candidate region is considered to be extracted based on the center of the macula.

Next, two methods namely multi-class Gaussian Bayes classifier and multi-SVM are used to classify other stages. Entire set of feature vector (f1-f11) determine the performance of both classifiers. In this paper, feature extraction is done manually for N training images.

## 4. Results

To perform quantitative and comparative analysis of DR grading, three different datasets are used namely Structured Analysis of Retina (STARE) [15], DIAbetic RETinopathy DataBase (DIARETDB1) [20], Digital Retinal Images for Vessel Extraction (DRIVE) and hospital database. STARE dataset contained 20 color images having a resolution of to 700×605 pixels, in which 10 images of them do not provide any pathology sign, taken by TopCon TRV-50 funds camera. While patients are aged between 25-90 years. DIARETDB1 dataset that includes 89 retinal images. These images have resolution of 1500X1152 pixels. Also they possess features related to noise and illumination. Moreover, in which five images considered do not pertain any DR lesions selected by medical experts and ground truth

provided by an expert by soft map. DRIVE dataset compose of 400 diabetic images, patients aged between 25-90 years in which, 33 images do not have any sign of DR. Each retinal image is taken using Canon CR5 camera and having a resolution of 768×584 pixels. The Table 1 summarizes the comprehensive specifications of the selected datasets.

Table 1. In depth specifications of the selected datasets, IVW: Illumination variation within images; IVA: Illumination variation across images.

Specifications	STARE	DIARETDB1	DRIVE
Cameras	Fixed	Fixed	Fixed
FOV	35	50	45
IVW	Normal	High	Normal
IVA	Normal	Low	Normal
Image Resolution	Fixed	Fixed	Fixed
Mydriatic	No	No	No

Furthermore, we implemented our proposed algorithm on a Corei-5(2.3-GHz PC) with 4GB of RAM. Moreover, in terms of time complexity our models usually converge is less than in a minute to diagnose DR in each stage.

Fifty percent of the dataset is selected at random for training, and remaining half is randomly selected for the testing purpose. In addition, performance is measured by using Sensitivity (Sen), Specificity (Spec) and Accuracy (Acc), which are defined as:

$$Sen = \frac{TP}{TP + FN} \tag{14}$$

$$Spec = \frac{TN}{TN + FP} \tag{15}$$

$$Acc = \frac{(TP+TN)}{(TP+TN+FP+FN)}$$
(16)

Where *TP*,*TN*,*FP*, and *FN* to stand for True Positive, False Positive, True Negative and False Negative respectively.

For grading of normal and severe stages DR, the statistical information on databases is tested as follows:

$$I(x_m, y_m) = \begin{cases} Normal, & p < t \\ Sever, & p > t \end{cases}$$
(17)

Where, P is known as mean, standard deviation and sum of the macula region having 100\*100 region and t is the threshold. Equation (12) classifies all the information generated by Equation (17). The accuracy of classification results of normal to severe is up to 99% and 98% respectively.

Tables 2, 3, 4, and 5 show the analysis of three different databases.

Table 2. Performance evaluation of DR grading at the various stages on DRIVE dataset.

Stages	Multi-c	lass Gaussi Exudates	ian Bayes	Multi-class SVM Exudates		
	Sen%	Spec%	Acc%	Sen%	Spec%	Acc%
Normal	100	97	99	100	98	99
Mild	90	94	95	94	96	97
Moderate	89	97	96	92	95	96
Severe	99	96	97	99	97	98

Table 3. Performance evaluation of DR grading at different stages on DIARETDB1 dataset.

Stages	Multi-class Gaussian Bayes Exudates			Multi-class SVM Exudates		
_	Sen%	Spec%	Acc%	Sen%	Spec%	Acc%
Normal	100	96	99	100	97	99
Mild	90	93	96	94	95	96
Moderate	89	95	97	91	94	96
Severe	99	95	96	99	97	98

Table 4. Performance evaluation of DR grading at different stages on Hospital database.

Stages	Multi-class Gaussian Bayes Exudates			Multi-class SVM Exudates		
	Sen%	Spec%	Acc%	Sen%	Spec%	Acc%
Normal	100	98	99	100	97	99
Mild	93	96	95	95	97	97
Moderate	91	97	96	92	95	96
Severe	96	98	98	99	98	98

Table 5. Performance evaluation of DR grading at different stages on STARE dataset.

Stages	Multi-class Gaussian Bayes Exudates			Multi-class SVM Exudates		xudates
	Sen%	Spec%	Acc%	Sen%	Spec%	Acc%
Normal	100	97	99	100	97	99
Mild	90	93	96	93	95	96
Moderate	90	95	96	92	93	94
Severe	99	95	96	99	96	97

In the next experimentation, the proposed method is compared with the prevailing DR grading methods. Often the comparisons are complex because of the use of dissimilar frameworks by the researchers. The performance comparison clearly indicates that the presented architecture yields better results with respect to other existing methods for MA detection. Tables 6 and 7 show the assessment of our method on with prevailing methods for MA and EXs detection.

Table 6. Proposed method and other techniques for MAs performance comparison.

	Sen%	Spec%	Acc%
Akram et al. [2]	98.6	99.69	99.40
Niemeijer et al. [30]	100	87	-
Fleming et al. [7]	85.4	83.1	-
Walter et al. [47]	88.5	-	-
Keerthi et al. [19]	88.46	-	-
Larsen et al. [22]	71.4	96.7	82.6
Multi-class SVM	98.86	99.74	99.42
Multi-class Gaussian Bayes	95.1	97.3	97.60

Table 7. Proposed method and earlier techniques for EXs, a performance comparison.

	Sen%	Spec%	Acc%
Akram et al. [3]	97.39	98.02	97.56
Ranamuka and	81.75	100.00	99.84
Meegama [35]			
Sinthanayothin et al.	88.5	99.7	-
[40]			
Clara et al. [19]	90.2	90	-
Niemeijer et al. [30]	95.0	86.0	-
Osareh et al. [32]	93	94.1	93.4
Walter et al. [47]	92.74	100	96.7
Multi-class SVM	96.64	98.69	99.40
Multi-class Gaussian Bayes	95.8	98.3	97.60

The level lesion experiment on different datasets is performed further. Multi-class Gaussian Bayes classifier does this analysis. Tables 8 and 9 show the EXs and MAs classification results on various datasets. The results are obtained on deep pixels analysis of images. For Ex and MAs labeling, the deep pixels analysis is done through CFT and then multi-class Gaussian Bayes classifier is applied for dark and bright labeling. It is revealed from the analysis that EXs are more accurately detected than MAs.

Table 8. Performance evaluation of Exudates (EXs) on hospital database.

Databasa	Exudates (EXs)				
Database	Sen%	Spec%	Acc%		
DB1	94	96	97		
DB2	93	95	96		
DB3	96	97	98		

Table 9. Performance evaluation of MAs/ HMAs on hospital database.

Databasa	MAs/ HMAs)				
Database	Sen%	Spec%	Acc%		
DB1	93	95	96		
DB2	92	95	94		
DB3	95	93	96		

### **5.** Conclusions

This research work proposes a preprocessing and feature extraction method to classify the DR at different stages. Preprocessing is an essential step at lesion level image segmentation for DR classification. CLAHE and ICA are combined for the preprocessing of retinal digital. Further, in the stat-of-art methods, Gaussian Curve Fitting technique is extended with thresholding technique for vessels extraction, ODN, and lesion detection. To strengthen the reliability, eleven different features are ensemble for the accurate classification of normal and abnormal retinal images. For classification purpose, multi-class Gaussian Bayes classifier and multi-SVM were used. The proposed approach is validated on two publically available databases namely STARE, DRIVE, DIARETDB1 and one hospital database collected by the authors. The average accuracy of both classifiers is better on normal to severe stages as compared to mild to moderate stages. Collectively results are shown in the results section.

## References

- Adali T., Anderson M., and Fu G., "Diversity in Independent Component and Vector Analyses: Identifiability, Algorithms, and Applications in Medical Imaging," *IEEE Signal Processing Magazine*, vol. 31, no. 3, pp. 18-33, 2014.
- [2] Akram M., Khalid S., and Khan S., "Identification and Classification of Microaneurysms for Early Detection of Diabetic Retinopathy," *Pattern Recognition*, vol. 46, no. 1, pp. 107-116, 2013.
- [3] Akram M., Khalid S., Tariq A., Khan S., and Azam F., "Detection and Classification of Retinal Lesions for Grading of Diabetic

Retinopathy," *Computers in Biology and Medicine*, vol. 45, pp. 161-171, 2014.

- [4] Akram M. and Khan S., "Multilayered Thresholding-Based Blood Vessel Segmentation for Screening of Diabetic Retinopathy," *Engineering with Computers*, vol. 29, no. 2, pp. 165-173, 2013.
- [5] Antal B. and Hajdu A., "An Ensemble-Based System for Microaneurysm Detection and Diabetic Retinopathy Grading," *IEEE Transactions on Biomedical Engineering*, vol. 59, no. 6, pp. 1720-1726, 2012.
- Belhadi S. and Benblidia N., "Automated Retinal [6] Segmentation Using Vessel Entropic Thresholding Based Spatial Correlation Histogram of Grav Level Images," The International Arab Journal of Information Technology, vol. 12, no. 5, pp. 441-446, 2015.
- [7] Fleming A., Philip S., Goatman K., Olson J., and Sharp P., "Automated Microaneurysm Detection Using Local Contrast Normalization and Local Vessel Detection," *IEEE Transactions on Medical Imaging*, vol. 25, no. 9, pp. 1223-1232, 2006.
- [8] Frank R., "Diabetic Retinopathy," Progress in Retinal and Eye Research, vol. 14, no. 2, pp. 361-392, 1995.
- [9] Fujita H., Uchiyama Y., Nakagawa T., Fukuoka D., Hatanaka Y., Hara T., Lee G., Hayashi Y., Ikedo Y., and Gao X., "Computer-Aided Diagnosis: The Emerging of Three CAD Systems Induced by Japanese Health Care Needs," *Computer Methods and Programs in Biomedicine*, vol. 92, no. 3, pp. 238-248, 2008.
- [10] Giancardo L., Karnowski T., Tobin K., Meriaudeau F., and Chaum E., "Validation of Microaneurysm-Based Diabetic Retinopathy Screening Across Retina Fundus Datasets," in Proceedings of the 26<sup>th</sup> IEEE International Symposium on Computer-Based Medical Systems, Porto, pp. 125-130, 2013.
- [11] Giancardo L., Meriaudeau F., Karnowski T., Li Y., Garg S., Tobin K., and Chaum E., "Exudate-Based Diabetic Macular Edema Detection in Fundus Images Using Publicly Available Datasets," *Medical Image Analysis*, vol. 16, no. 1, pp. 216-226, 2012.
- [12] Hammes H., Lemmen K., and Bertram B., "Diabetic Retinopathy and Maculopathy," *Experimental and Clinical Endocrinology and Diabetes*, vol. 122, no. 7, pp. 387-390, 2014.
- [13] Hashim M. and Hashim S., "Comparison of Clinical and Textural Approach for Diabetic Retinopathy Grading," *IEEE International Conference on Control System, Computing and Engineering*, Penang, pp. 290-295, 2012.
- [14] Hasikin K. and Isa N., "Adaptive Fuzzy Contrast Factor Enhancement Technique for Low Contrast and Nonuniform Illumination Images," *Signal*,

Image and Video Processing, vol. 8, no. 8, pp. 1591-1603, 2014.

- [15] Hoover A., "STARE database," Available: Available: http://www. ces. clemson. edu/~ ahoover/stare, Last Visited, 2016.
- [16] Jadoon M., Dineen B., Bourne R., Shah S., Khan M., Johnson G., Gilbert C., and Khan M., "Prevalence of Blindness and Visual Impairment in Pakistan: the Pakistan National Blindness and Visual Impairment Survey," *Investigative Ophthalmology and Visual Science*, vol. 47, no. 11, pp. 4749-4755, 2006.
- [17] Jindal K., Gupta K., Jain M., and Maheshwari M., "Bio-Medical Image Enhancement Based on Spatial Domain Technique," in Proceedings of International Conference on Advances in Engineering and Technology Research, Unnao, pp. 1-5, 2014.
- [18] Jitpakdee P., Aimmanee P., and Uyyanonvara B., "A Survey on Hemorrhage Detection in Diabetic Retinopathy Retinal Images," in Proceedings of 9<sup>th</sup> International Conference on Electrical Engineering/Electronics, Computer, Telecommunications and Information Technology, Phetchaburi, pp. 1-4, 2012.
- [19] Kahai P., Namuduri K., and Thompson H., "A Decision Support Framework for Automated Screening of Diabetic Retinopathy," *International Journal of Biomedical Imaging*, vol. 2006, pp. 8, 2006.
- [20] Kauppi T., Kalesnykiene V., Kamarainen J., Lensu L., Sorri I., Raninen A., Voutilainen R., Uusitalo H., Kälviäinen H., and Pietilä J., "The DIARETDB1 Diabetic Retinopathy Database and Evaluation Protocol," *in Proceedings of the British Machine Vision Conference*, UK, pp. 1-18, 2007.
- [21] Klein R., Myers C., Lee K., Gangnon R., and Klein B., "Changes in Retinal Vessel Diameter And Incidence and Progression of Diabetic Retinopathy," *Archives of Ophthalmology*, vol. 130, no. 6, pp. 749-755, 2012.
- [22] Larsen M., Godt J., Larsen N., Lund-Andersen H., Sjølie A., Agardh E., Kalm H., Grunkin M., and Owens D., "Automated Detection of Fundus Photographic Red Lesions in Diabetic Retinopathy," *Investigative Ophthalmology and Visual Science*, vol. 44, no. 2, pp. 761-766, 2003.
- [23] Lau A., Tang A., Chung B., Yeung P., Wei X., Chan B., Shum H., Wong K., and Tsia K., "High-Throughput Image-Based Single-Cell Analysis by Ultrafast Asymmetric-Detection Time-Stretch Optical Microscopy," in of Bio-Optics: Proceedings Design and Application: Optical Society of America, Vancouver, pp. BW1A. 4, 2015.

- [24] Meyer-Baese A. and Schmid V., *Pattern Recognition and Signal Analysis in Medical Imaging*, Elsevier, 2014.
- [25] Mookiah M., Acharya U., Chua C., Lim C., Ng E., and Laude A., "Computer-Aided Diagnosis of Diabetic Retinopathy: A Review," *Computers in Biology and Medicine*, vol. 43, no. 12, pp. 2136-2155, 2013.
- [26] Mubbashar M., Usman A., and Akram M., "Automated System for Macula Detection In Digital Retinal Images," in Proceedings of International Conference on Information and Communication Technologies, Karachi, pp. 1-5, 2011.
- [27] Murray V., Agurto C., Barriga S., Pattichis M., and Soliz P., "Real-time Diabetic Retinopathy Patient Screening Using Multiscale AM-FM Methods," in Proceedings of 19<sup>th</sup> IEEE International Conference on Image Processing, Orlando, pp. 525-528, 2012.
- [28] Niemeijer M., Abramoff M., and Ginneken B., "Image Structure Clustering for Image Quality Verification of Color Retina Images in Diabetic Retinopathy Screening," *Medical Image Analysis*, vol. 10, no. 6, pp. 888-898, 2006.
- [29] Niemeijer M., Staal J., Van Ginneken B., Loog M., and Abramoff M., "Comparative Study of Retinal Vessel Segmentation Methods on A New Publicly Available Database," in Proceedings of Medical Imaging International Society for Optics and Photonics, San Diego, pp. 648-656, 2004.
- [30] Niemeijer M., Van Ginneken B., Cree M., Mizutani A., Quellec G., Sánchez C., Zhang B., Hornero R., Lamard M., Muramatsu C., Wu X., Cazuguel G., You J., Mayo A., Li Q., Hatanaka Y., Cochener B., Roux C., Karray F., Garcia M., Fujita H., and Abramoff M., "Retinopathy Online Challenge: Automatic Detection of Microaneurysms in Digital Color Fundus Photographs," *IEEE Transactions on Medical Imaging*, vol. 29, no.1, pp. 185-195, 2010.
- [31] Orton E., Forbes-Haley A., Tunbridge L., and Cohen S., "Equity of Uptake of A Diabetic Retinopathy Screening Programme in A Geographically and Socio-Economically Diverse Population," *Public Health*, vol. 127, no. 9, pp. 814-821, 2013.
- [32] Osareh A., Mirmehdi M., Thomas B., and Markham R., "Automated Identification of Diabetic Retinal Exudates in Digital Colour Images," *British Journal of Ophthalmology*, vol. 87, no.10, pp. 1220-1223, 2003.
- [33] Qureshi R., Kovacs L., Harangi B., Nagy B., Peto T., and Hajdu A., "Combining Algorithms for Automatic Detection of Optic Disc and Macula in Fundus Images," *Computer Vision and Image Understanding*. vol. 116, no. 1, pp. 138-145, 2012.

- [34] Raja S. and Vasuki S., "Screening Diabetic Retinopathy in Developing Countries using Retinal Images," *Applied Medical Informatic*, vol. 36, no. 1, pp. 13-22, 2015.
- [35] Ranamuka N. and Meegama R., "Detection of Hard Exudates from Diabetic Retinopathy Images Using Fuzzy Logic," *IET Image Processing*, vol. 7, no. 2, pp. 121-130, 2013.
- [36] Singh R., Roy S., and Singh M., "Histogram Domain Adaptive Power Law Applications in Image Enhancement Technique," *International Journal of Computer Science and Information Technologies*, vol. 5, no. 3, pp. 3972-3978, 2014.
- [37] Saleh M. and Eswaran C., "An Automated Decision-Support System for Non-Proliferative Diabetic Retinopathy Disease Based on Mas and Has Detection," *Computer Methods and Programs in Biomedicine*, vol. 108, no. 1, pp. 186-196, 2012.
- [38] Sánchez C., Niemeijer M., Išgum I., Dumitrescu A., Suttorp-Schulten M., Abràmoff M., and Van Ginneken B., "Contextual Computer-Aided Detection: Improving Bright Lesion Detection in Retinal Images and Coronary Calcification Identification in CT Scans," *Medical Image Analysis*, vol. 16, no. 1, pp. 50-62, 2012.
- [39] Sharma P., Nirmala S., and Sarma K., "A System for Grading Diabetic Maculopathy Severity Level," *Network Modeling Analysis in Health Informatics and Bioinformatics*, vol. 3, no. 1, pp. 1-9, 2014.
- [40] Sinthanayothin C., Boyce J., Williamson T., Cook H., Mensah E., Lal S., and Usher D., "Automated Detection of Diabetic Retinopathy On Digital Fundus Images," *Diabetic Medicine*, vol. 19, no. 2, pp. 105-112, 2002.
- [41] Sonka M., Hlavac V., and Boyle R., *Image Processing, Analysis, and Machine Vision:* Cengage Learning, 2014.
- [42] Sopharak A., Uyyanonvara B., Barman S., and Williamson T., "Automatic Detection of Diabetic Retinopathy Exudates from Non-Dilated Retinal Images Using Mathematical Morphology Methods," *Computerized Medical Imaging and Graphics*, vol. 32, no. 8, pp. 720-727, 2008.
- [43] Sree V. and Rao P., "Hardware Implementation of Enhancement of Retinal Fundus Image Using Simulink," in Proceedings of IEEE Asia Pacific Conference on Postgraduate Research in Microelectronics and Electronics (PrimeAsia), Visakhapatnam, pp. 239-244, 2013.
- [44] Staal J., Abràmoff M., Niemeijer M., Viergever M., and Van Ginneken B., "Ridge-Based Vessel Segmentation in Color Images of The Retina," *IEEE Transactions on Medical Imaging*, vol. 23, no. 4, pp. 501-509, 2004.

- [45] Tariq A., Akram M., and Javed M., "Computer Aided Diagnostic System for Grading of Diabetic Retinopathy," in Proceedings of 4<sup>th</sup> International Workshop on Computational Intelligence in Medical Imaging, Singapore, pp. 30-35, 2013.
- [46] Thamman P., Purcitm P., and Verma A., "Contrast Enhancement of Medical Images-A Review," *International Journal of Innovations and Advancement in Computer Science*, vol. 3, no. 4, pp. 124-128, 2014.
- [47] Walter T., Massin P., Erginay A., Ordonez R., Jeulin C., and Klein J., "Automatic Detection of Microaneurysms in Color Fundus Images," *Medical Image Analysis*, vol. 11, no. 6, pp. 555-566, 2007.
- [48] Watkins P., "ABC of Diabetes: Retinopathy," *British Medical Journal*, vol. 326, no. 7395, pp. 924-926, 2003.
- [49] Wendt G., Screening for Diabetic Retinopathy Aspects of Photographic Methods, Thesis, Karolinska Institutet, 2005.
- [50] Yadav G., Maheshwari S., and Agarwal A., "Contrast Limited Adaptive Histogram Equalization Based Enhancement for Real Time Video System," *in Proceedings of International Conference on Advances in Computing, Communications and Informatics*, New Delhi, pp. 2392-2397, 2014.
- [51] Yun W., Rajendra Acharya U., Venkatesh Y., Chee C., Min L., and Ng E., "Identification of Different Stages of Diabetic Retinopathy Using Retinal Optical Images," *Information Sciences*, vol. 178, no. 1, pp. 106-121, 2008.



**Muhammad Sharif** Ph.D., is Associate Professor at COMSATS, Wah Cantt Pakistan. His area of specialization is Artificial Intelligence and Image Processing. He is into teaching field from 1995 till date. He has 110 plus research

publications in IF, SCI and ISI journals, national and international conferences. Up till now he has supervised 25 MS(CS) thesis. He is currently supervising 5 Ph.D.(CS) students and co-supervisor of 5 others. More than 200 undergraduate students had already been passed out after successful completion of their project work under his supervision. His research interests are Image Processing, Computer Networks & Security, and Algorithms Design and Analysis.



Jamal Hussain Shah is a Ph.D. Scholar at University of Science and Technology of China (USTC), China. He is graduated from COMSATS Institute of Information Technology, Pakistan in 2011. His areas of interest are Digital Image

Processing and Networking. Mr. Jamal has more than five years of experience of teaching and IT related projects.